

# Package ‘clintools’

January 20, 2022

**Type** Package

**Title** Tools for Clinical Research

**Version** 0.9.2

**Description** Every research team have their own script for data management, statistics and most importantly hemodynamic indices. The purpose is to standardize scripts utilized in clinical research. The hemodynamic indices can be used in a long-format dataframe, and add both periods of interest (trigger-periods), and delete artifacts with deleter-files. Transfer function analysis (Claassen et al. (2016) <[doi:10.1177/0271678X15626425](https://doi.org/10.1177/0271678X15626425)>) and Mx (Czosnyka et al. (1996) <[doi:10.1161/01.str.27.10.1829](https://doi.org/10.1161/01.str.27.10.1829)>) can be calculated using this package.

**License** MIT + file LICENSE

**URL** <https://github.com/lilleoel/clintools>

**BugReports** <https://github.com/lilleoel/clintools/issues>

**Depends** R (>= 3.5.0)

**Encoding** UTF-8

**Language** en-US

**LazyData** true

**RoxygenNote** 7.1.1

**Suggests** knitr, rmarkdown

**Imports** signal (>= 0.7-6), xml2 (>= 1.3.2), lme4 (>= 1.1-27.1)

**NeedsCompilation** no

**Author** Markus Harboe Olsen [cre, aut],  
Christian Riberholt [aut],  
Ronan Berg [aut],  
Kirsten Moeller [aut]

**Maintainer** Markus Harboe Olsen <[oel@oelfam.com](mailto:oel@oelfam.com)>

**Repository** CRAN

**Date/Publication** 2022-01-20 15:52:43 UTC

## R topics documented:

clinmon	2
df.data1000	6
df.deleter	7
iscus	7
ortable	8
PLR3000	9
rrGcomp	9
sRCT	10
testdata10	11
TFA	12
tfa_sample_data	16
tfa_sample_data_1	17
tfa_sample_data_2	18

<b>Index</b>	<b>19</b>
--------------	-----------

---

clinmon	<i>Hemodynamic Indices Calculated From Clinical Monitoring (clinmon)</i>
---------	--

---

### Description

clinmon() uses a *continuous* recording and returns a dataframe with hemodynamic indices for every period, epoch or block depending on the input. Calculates COest, CPPopt, CVRi, Dx, Mx, PI, PRx, PWA, RI, and Sx (see *Hemodynamic indices*).

### Usage

```
clinmon(df, variables,
        trigger = NULL, deleter = NULL,
        blocksize = 3, epochsize = 20,
        overlapping = FALSE, freq = 1000,
        blockmin = 0.5, epochmin = 0.5,
        output = "period", fast = FALSE)
```

### Arguments

df	Raw <i>continuous</i> recording with all numeric data and first column has to be time in seconds. (dataframe)
variables	Defining the type and order of the recorded variables as a list. Middle cerebral artery blood velocity ('mcav'), Arterial blood pressure ('abp'), cerebral perfusion pressure ('cpp'), intracranial pressure ('icp'), and heart rate ('hr') is currently supported. <i>It is necessary that time is the first row.</i> (list)
trigger	Trigger with two columns: first is start, and second is end of periods to be analyzed. Every row corresponds to a period. Default is NULL, which results in analysis of the full dataframe. (dataframe)

deleter	Deleter with two columns: first is start and second is end of period with artefacts, which need to be deleted. Every row is a period with artefacts. Default is NULL. (dataframe)
blocksize	Length of a block, in seconds. Default is 3. (numeric)
epochsize	Size of epochs in number of blocks. Default is 20. (numeric)
overlapping	The number of block which should overlap when calculating correlation based indices, and remain blank if overlapping calculations should not be utilized. Default is FALSE. (numeric)
freq	Frequency of recorded data, in Hz. Default is 1000. (numeric)
blockmin	Minimum measurements required to create a block in ratio. Default is 0.5 corresponding to 50%. If the block holds less than the defined ratio the block will be omitted. (numeric)
epochmin	Minimum number of blocks required to create an epoch in ratio. Default is 0.5 corresponding to 50%. If the epoch holds less than the defined ration the epoch will be omitted. (numeric)
output	Select what each row should represent in the output. Correlation based indices are not presented when selecting blocks for every row. Currently 'block', 'epoch', 'period' or 'cpropt' is supported. Default is 'period'. (string)
fast	Select if you want the data to aggregated before analysis resulting in a faster, but perhaps more imprecise run, in Hz. Default is FALSE. (numeric)

## Details

Using a *continuous* raw recording, `clinmon()` calculates hemodynamic indices for every period, epoch or block depending on the chosen output.

View(data)

```

      time  abp  mcav
      7.00   78   45
      7.01   78   46
      ...   ...   ...
    301.82   82   70
    301.83   81   69

```

To calculate the indices insert the data and select the relevant variables.

```
clinmon(df=data, variables=c("abp", "mcav"))
```

See **Value** for output description.

## Value

Returns a dataframe with the results, with either every blocks, epochs or periods as rows, depending on the chosen output.

The columns of the output are:

- period - The period number corresponding to the row-number in the trigger file.
- epoch - The epoch number, or if period is chosen as output it reflects the number of epochs in the period.
- block - The block number, or if period or epoch is chosen as output it reflects the number of blocks in the period or epoch.
- time\_min - The minimum time value of the period, epoch or block.
- time\_max - The maximum time value of the period, epoch or block.
- missing\_percent - The percentage of missing data in the period, epoch or block.
- XX\_mean - The mean value of each variable for the period, epoch or block.
- XX\_min - The minimum value of each variable for the period, epoch or block.
- XX\_max - The maximum value of each variable for the period, epoch or block.
- YY - The indices in each column.

### Hemodynamic indices

#### COest | **Estimated cardiac output:**

*Required variables:* abp, hr; *Required output:* -.

Estimated cardiac output (COest) is calculated by utilizing the method described by Koenig et al. [1]:

$$COest = PP / (SBP + DBP) * HR$$

PP: Pulse pressure; SBP: systolic blood pressure; DBP: diastolic blood pressure; HR: heart rate.

#### CPPopt | **Optimal cerebral perfusion pressure:**

*Required variables:* abp, icp; *Required output:* period.

Optimal cerebral perfusion pressure (CPPopt) is calculated utilizing the method described by Steiner et al. [2]. The CPPopt return NA if CPPopt is the maximum or minimum CPP investigated. CPPopt is recommended to only be calculated after 'several hours' of recording:

$$CPPopt = The5mmHgCPPIntervalWithLowestMeanPRx$$

CPP: cerebral perfusion pressure; PRx: Pressure reactivity index.

#### CVRi | **Cardiovascular resistance index:**

*Required variables:* abp, mcav; *Required output:* -.

Cardiovascular resistance index (CVRi) is calculated utilizing the method described by Fan et al. [3]:

$$CVRi = meanABP / meanMCAv$$

ABP: arterial blood pressure; MCAv: middle cerebral artery blood velocity.

#### Dx | **Diastolic flow index:**

*Required variables:* cpp/abp, mcav; *Required output:* epoch, period.

Diastolic flow index (Dx) is calculated utilizing the method described by Reinhard et al. [4]:

$$Dxc = cor(meanCPP / minMCAv)$$

$$Dxa = cor(meanABP/minMCAv)$$

cor: correlation coefficient; CPP: cerebral perfusion pressure; ABP: arterial blood pressure; MCAv: middle cerebral artery blood velocity.

**Mx | Mean flow index:**

*Required variables:* cpp/abp, mcav; *Required output:* epoch, period.

Mean flow index (Mx) is calculated utilizing the method described by Czosnyka et al. [5]:

$$Mxc = cor(meanCPP/meanMCAv)$$

$$Mxa = cor(meanABP/meanMCAv)$$

cor: correlation coefficient; CPP: cerebral perfusion pressure; ABP: arterial blood pressure; MCAv: middle cerebral artery blood velocity.

**PI | Gosling index of pulsatility:**

*Required variables:* mcav; *Required output:* -.

Gosling index of pulsatility (PI) is calculated utilizing the method described by Michel et al. [6]:

$$PI = (systolicMCAv - diastolicMCAv)/meanMCAv$$

MCAv: middle cerebral artery blood velocity.

**PRx | Pressure reactivity index:**

*Required variables:* abp, icp; *Required output:* epoch, period.

Pressure reactivity index (PRx) is calculated utilizing the method described by Czosnyka et al. [7]:

$$PRx = cor(meanABP/meanICP)$$

cor: correlation coefficient; CPP: cerebral perfusion pressure; ICP: intracranial pressure.

**PWA | Pulse wave amplitude:**

*Required variables:* cpp/icp/abp/mcav; *Required output:* -.

Pulse wave amplitude (PWA) is calculated utilizing the method described by Norager et al. [8]:

$$PWA = systolic - diastolic$$

**RI | Pourcelots resistive (resistance) index:**

*Required variables:* mcav; *Required output:* -.

Pourcelots resistive (resistance) index (RI) is calculated utilizing the method described by Forster et al. [9]:

$$RI = (systolicMCAv - diastolicMCAv)/systolicMCAv$$

MCAv: middle cerebral artery blood velocity.

**Sx | Systolic flow index:**

*Required variables:* cpp/abp, mcav; *Required output:* epoch, period.

Systolic flow index (Sx) is calculated utilizing the method described by Czosnyka et al. [5]:

$$Sxc = cor(meanCPP/systolicMCAv)$$

$$Sxa = cor(meanABP/systolicMCAv)$$

cor: correlation coefficient; CPP: cerebral perfusion pressure; ABP: arterial blood pressure; MCAv: middle cerebral artery blood velocity.

## References

1. Koenig et al. (2015) Biomed Sci Instrum. 2015;51:85-90. ([PubMed](#))
2. Steiner et al. (2002) Crit Care Med. 2002 Apr;30(4):733-8. ([PubMed](#))
3. Fan et al. (2018) Front Physiol. 2018 Jul 16;9:869. ([PubMed](#))
4. Reinhard et al. (2003) Stroke. 2003 Sep;34(9):2138-44. ([PubMed](#))
5. Czosnyka et al. (1996) Stroke. 1996 Oct;27(10):1829-34. ([PubMed](#))
6. Michel et al. (1998) Ultrasound Med Biol. 1998 May;24(4):597-9. ([PubMed](#))
7. Czosnyka et al. (1997) Neurosurgery. 1997 Jul;41(1):11-7; discussion 17-9. ([PubMed](#))
8. Norager et al. (2020) Acta Neurochir (Wien). 2020 Dec;162(12):2983-2989. ([PubMed](#))
9. Forster et al. (2017) J Paediatr Child Health. 2018 Jan;54(1):61-68. ([PubMed](#))

## Examples

```
data(testdata)
clinmon(df.data10, variables=c('abp', 'mcav', 'hr'), freq=10)
```

---

df.data1000

*Test-data - 1000 Hz*

---

## Description

Recording with four columns: time (t), non-invasive arterial blood pressure (abp), middle cerebral artery velocity measured using transcranial Doppler (mcav), and heart rate (hr).

## Usage

```
data(testdata)
```

## Format

An object of class "dataframe"; an example of the usage in [clinmon](#)-function.

## References

Olsen MH et al. (Unpublished data, 2020) ([GitHub](#))

## Examples

```
data(testdata)
variables <- c("abp", "mcav", "hr")
clinmon(df.data1000, variables, fast=50)
```

---

`df.deleter`*Test-deleter*

---

**Description**

Deleter dataframe with two columns: start (start) and end (end) of the deleter-period.

**Usage**

```
data(testdata)
```

**Format**

An object of class "dataframe"; an example of the usage in `clinmon`-function.

**References**

Olsen MH et al. (Unpublished data, 2020) ([GitHub](#))

**Examples**

```
data(testdata)
variables <- c("abp", "mcav", "hr")
clinmon(df.data1000, variables, deleter=df.deleter, fast=50)
```

---

`iscus`*ISCUSFlex-values to dataframe (iscus)*

---

**Description**

`iscus()` is a function which converts XML files extracted from the Microdialysis-apparatur of ISCUSFlex apparatus to a dataframe.

**Usage**

```
iscus(filename)
```

**Arguments**

`filename` path to the XML-file with the measurements

**Value**

Returns a dataframe with the measurements.

**Examples**

```
## Not run:
iscus("C:/ISCUSfiles/7888e844-1c7a-40af-a3f2-3bb27a8dd9e5.xml")

## End(Not run)
```

---

ortable

*Logistic regression table with Odds ratio (ortable)*


---

**Description**

ortable() is a small function which utilises the output from the glm-function to print a dataframe with odds ratio, confidence limits, and p-values.

**Usage**

```
ortable(x, d, d_p, intercept, simple)
```

**Arguments**

x	Utilises the output from a glm-function. (glm-output)
d	Refers to the number of digits for odds ratio and confidence intervals. Default is 2. (numeric)
d_p	Refers to the number of digits for odds ratio and confidence intervals. Default is 3. (numeric)
intercept	The intercept is presented in the table if TRUE. Default is FALSE. (boolean)
simple	Odds ratio and confidence intervals are merged into one column if TRUE. Default is TRUE. (boolean)

**Value**

Returns a dataframe with with odds ratio, confidence limits, and p-values.

**Examples**

```
df <- data.frame(outcome=sample(0:1, 100,replace=TRUE),
                 var=sample(0:100,100,replace=TRUE))
ortable(glm(outcome ~ ., data=df))
```



---

PLR3000	<i>NeurOpticsTM PLR-3000 pupillometer file to dataframe (PLR3000)</i>
---------	---

---

### Description

PLR3000() is a function which converts the XLS file imported from the eurOpticsTM PLR-3000 pupillometer to a nested list with two dataframes.

### Usage

```
PLR3000(filename = NULL, df = NULL)
```

### Arguments

filename	path to the XLS-file with the measurements
df	the dataframe can also be used for the function if data is already imported.

### Value

Returns a list with two dataframe, one with the measurements (pupils) and one with the markers (markers).

### Examples

```
## Not run:  
PLR3000("C:/PLR3000/R_20200105_205901.xls")  
  
## End(Not run)
```

---

rrGcomp	<i>Relative risk derived by G-computation (rrGcomp)</i>
---------	---

---

### Description

rrGcomp() is a small function which generates population-level (marginal) relative risks derived by G-computation. For models with random effects mixed-effects generalized linear model with a logit link with adjustment for stratification variables will be used, while those without random effects a logistic regression will be used. The code is based on the method used in the paper by Dankiewicz et al. (2021) N Engl J Med. Jun 17;384(24):2283-2294. ([PubMed](#))

### Usage

```
rrGcomp(df, outcome_col, group_col,  
fixed_strata = NULL, random_strata = NULL,  
nbrIter = 5000, conf_level = 0.95)
```

**Arguments**

df	the individual participant dataframe
outcome_col	column name for the outcome column
group_col	column name for the group column
fixed_strata	list of column names for the fixed effect stratification columns
random_strata	list of column names for the random effect stratification columns
nbrIter	number of iterations to be used in the G-computation. The original paper used 5000, which is also the default.
conf_level	the confidence level to be reported.

**Value**

Returns a list with relative risk (rr), simulated rr (simRR), lower- and upper confidence level (simLCL/simUCL), and the p-value (p\_val)

**Examples**

```
df <- sRCT(n_sites=3,n_pop=50)
rrGcomp(df,"outcome","Var1","age","site",10)
```

---

sRCT

*simulated Randomised Clinical Trial (sRCT)*


---

**Description**

sRCT() is a function which simulates a randomised clinical trial with a binary outcome and returns a dataframe. This version is validated to be used for analysis of interaction in a factorial design.

**Usage**

```
sRCT(part_tbl = NULL, all_sizes = NULL,
n_pop = 100,n_sites = 1,design = c(2,2,2),
rrr = c(0.05,0.05,0), interaction = c(`1<-2` = 0.05, `1<>2` = -0.05),
strata_var = c("age","sex"), strata_site = T,
strata_risk = c(age=0.3,sex=0.5),
outcome_risk = 0.492)
```

**Arguments**

part_tbl	Here a participation data frame should be imported. [TODO: NOT FUNCTIONAL]
all_sizes	Size of blocks in allocation table. If left empty the three lowest possible block sizes will be randomly assigned.
n_pop	Number of participants included in the trial.

n_sites	Number of sites
design	Number of sites as a list where each element corresponds to an intervention and the number in the element is the number of groups. So for a 2x2 factorial design <code>c(2, 2)</code> should be used. [TODO: THREE GROUPS]
rrr	relative risk reduction for each intervention so for the abovementioned 2x2 factorial desing with RRR of 0.05 and 0.10 we would use <code>c(0.05, 0.10)</code> .
interaction	Interaction between interventions with a named list. If intervention 2 increases the RRR of intervention 1 we would use <code>1&lt;-2 = 0.05</code> .
strata_var	Variable which would be used for stratification.
strata_site	If randomisation should be stratified by site
strata_risk	The frequency of a dichotomised strata. Named list where the name must correspond to a strata var.
outcome_risk	The baseline risk of the dichotomous primary outcome.

### Details

The sRCT function is continuously being developed to answer specific questions in simulation studies. sRCT will be updated and tested for each specific question. For each update the function will be validated for the current purpose and all previous purposes. sRCT is not validated for all simulation studies

### Value

Returns a dataframe with an individual participant data frame.

### Examples

```
sRCT()
```

---

testdata10

*Test-data - 10 Hz*

---

### Description

Recording with four columns: time (t), non-invasive arterial blood pressure (abp), middle cerebral artery velocity measured using transcranial Doppler (mcav), and heart rate (hr).

### Usage

```
data(testdata)
```

### Format

An object of class "dataframe"; an example of the usage in [clinmon](#)-function.

## References

Olsen MH et al. (Unpublished data, 2020) ([GitHub](#))

## Examples

```
data(testdata)
variables <- c("abp", "mcav", "hr")
clinmon(df.data10, variables, freq=10)
```

---

TFA

*Transfer function analysis of dynamic cerebral autoregulation (TFA)*


---

## Description

TFA() calculates dynamic cerebral autoregulation through a transfer function analysis from a *continuous* recording. This function follows the recommendations from Claassen et al. [1] and mimicks the matlab script created by David Simpsons in 2015 ([Matlab TFA function](#)). TFA() also includes the possibility to analyse raw recordings with application of cyclic (beat-to-beat) average with the possibility of utilizing interpolation. (see **details**).

## Usage

```
TFA(df, variables,
    trigger = NULL, deleter = NULL,
    freq = 1000, fast = 50, raw_data = FALSE,
    interpolation = 3, output = "table",
    vlf = c(0.02, 0.07), lf = c(0.07, 0.2),
    hf = c(0.2, 0.5), detrend = FALSE,
    spectral_smoothing = 3,
    coherence2_thresholds = cbind(c(3:15),
    c(0.51, 0.40, 0.34, 0.29, 0.25, 0.22, 0.20, 0.18,
    0.17, 0.15, 0.14, 0.13, 0.12)),
    apply_coherence2_threshold = TRUE,
    remove_negative_phase = TRUE,
    remove_negative_phase_f_cutoff = 0.1,
    normalize_ABP = FALSE,
    normalize_CBFV = FALSE,
    window_type = 'hanning',
    window_length = 102.4,
    overlap = 59.99,
    overlap_adjust = TRUE,
    na_as_mean = TRUE)
```

**Arguments**

df	Raw <i>continuous</i> recording with numeric data and first column has to be time in seconds. (dataframe)
variables	Definition of the type and order of recorded variables as a list. Middle cerebral artery blood velocity ('mcaV') and arterial blood pressure ('abp') is currently supported. (list)
trigger	Trigger with two columns: first is start, and second is end of period to be analyzed. Every row is a period for analysis. Default is NULL, which results in analysis of the full dataframe. (dataframe)
deleter	Deleter with two columns: first is start and second is end of period with artefacts, which need to be deleted. Every row is a period with artefacts. Default is NULL. (dataframe)
freq	Frequency of recorded data, in Hz. Default is 1000. (numeric)
fast	Select if you want the data to aggregated resulting in a faster, but perhaps more imprecise run, in Hz. Default is 50 (numeric)
raw_data	Select TRUE if the data is raw and cyclic mean should be calculated. <b>NB:</b> this function have not been validated, why validated methods for calculating cyclic mean are preferred. Only 1 period can be analysed using raw_data. Default is FALSE (boolean)
interpolation	Select the number of beats which should be interpolated. Default is up to 3 beats and 0 results in no interpolation. (numeric)
output	Select what the output should be. 'table' results in a dataframe with values for the three frequencies defined by Claassen et al. [1]; 'long' results in a dataframe with the results in a long format; 'plot' results in a dataframe which can help plot gain, phase and coherence; 'plot-peak' results in a dataframe, which can be used to validate the cyclic average, and 'raw' results in a nested list with results primarily for debugging. Default is 'table'. (string)
vlf, lf, hf, detrend, spectral_smoothing, coherence2_thresholds	See <b>TFA-parameters</b>
apply_coherence2_threshold, remove_negative_phase	See <b>TFA-parameters</b>
remove_negative_phase_f_cutoff, normalize_ABP	See <b>TFA-parameters</b>
normalize_CBFV, window_type, window_length, overlap	See <b>TFA-parameters</b>
overlap_adjust, na_as_mean	See <b>TFA-parameters</b>

**Details**

Using a *continuous* raw recording, TFA() calculates dynamic cerebral autoregulation trough a transfer function analysis. This function utilizes the recommendations from Claassen et al [1] and mimicks the matlab script created by David Simpsons in 2015.

View(data)

time	abp	mcav
7.00	78	45
7.01	78	46
...	...	...
301.82	82	70
301.83	81	69

To calculate the variables insert the data and select the relevant variables.

```
TFA(df=data, variables=c("abp", "mcav"))
```

See **Value** for output description.

### Value

TFA() returns a dataframe depending on the output selected. 'table' results in a dataframe with values for the three frequencies defined by Claassen et al. [1]; 'long' results in a dataframe with the results in a long format; 'plot' results in a dataframe which can help plot gain, phase and coherence; 'plot-peak' results in a dataframe, which can be used to validate the cyclic average, and 'raw' results in a nested list with results primarily for debugging.

Some generic variables are listed below:

- abp\_power - The blood pressure power measured in  $\text{mmHg}^2$ .
- cbfv\_power - The cerebral blood flow velocity power measured in  $\text{cm}^2 \text{s}^{-2}$ .
- coherence - Coherence.
- gain\_not\_normal - Not normalized gain measured in  $\text{cm} \text{s}^{-1} \text{mmHg}^{-1}$ .
- gain\_normal - Normalized gain measured in  $\% \text{mmHg}^{-1}$ .
- phase - Phase measured in radians.

#### output = 'table':

Wide format output table with period, VLF, LF, and HF as columns, and the TFA-variables as rows.

period	variable	vlf	lf	hf
1	abp_power	6.25	1.56	0.21
1	cbfv_power	3.22	2.25	0.30
...	...	...	...	...
3	gain_normal	1.04	1.48	1.85
3	phase	53.0	25.4	9.38

#### output = 'long':

Long format output table which can be manipulated depending on the intended use, with period, interval, variables and values as columns.

period	interval	variable	values
--------	----------	----------	--------

1	hf	abp_power	6.25
1	hf	cbfv_power	3.22
...	...	...	...
2	vlf	gain_norm	1.85
2	vlf	phase	9.38

**output = 'plot':**

Plot format output table which can be used to draw figures with gain, phase and coherence depending on frequency.

period	freq	gain	phase	coherence
1	0.00	0.16	0.00	0.04
1	0.01	0.29	4.22	0.29
...	...	...	...	...
2	1.55	1.15	-43.2	0.64
2	1.56	1.16	-41.1	0.42

**TFA-parameters**

A series of parameters that control TFA analysis (window-length, frequency bands ...). If this is not provided, default values, corresponding to those recommended in the white paper, will be used. These default values are given below for each parameter.

- **vlf** Limits of *very low frequency* band (in Hz). This corresponds to the mathematical inclusion of [X:Y]. Default is c(0.02-0.07).
- **lf** Limits of *low frequency* band (in Hz). This corresponds to the mathematical inclusion of [X:Y]. Default is c(0.07-0.2).
- **hf** Limits of *high frequency* band (in Hz). This corresponds to the mathematical inclusion of [X:Y]. Default is c(0.2-0.5).
- **detrend** Linear detrending of data prior to TFA-analysis (detrending is carried out as one continuous trend over the whole length of the recording, not segment-by-segment). Default is FALSE.
- **spectral\_smoothing** The length, in samples, of the triangular spectral smoothing function. Note that this must be an odd number, to ensure that smoothing is symmetrical around the centre frequency. Default is 3.
- **coherence2\_thresholds** The critical values (alpha=5%, second column) for coherence for a number of windows (first column, here from 3 to 15). These values were obtained by Monte Carlo simulation, using the default parameter settings for the TFA-analysis (Hanning window, overlap of 50% and 3-point spectral smoothing was assumed). These values should be recalculated for different settings. Note that if `overlap_adjust=TRUE`, the overlap will vary depending on the length of data. With an overlap of 60% (see below), the critical values increase by between 0.04 (for 3 windows) and 0.02 (for 15 windows). Default is `cbind(c(3:15),c(0.51,0.40, 0.34,0.29,0.25,0.22,0.20,0.18,0.17, 0.15,0.14,0.13,0.12))`.
- **apply\_coherence2\_threshold** Apply the thresholds given above to the TFA-estimates. All frequencies with magnitude-squared coherence below the threshold value are excluded from

averaging when calculating the mean values of gain and phase across the bands. Note that low values of coherence are not excluded in the average of coherence across the bands. Default is TRUE.

- `remove_negative_phase` Remove (ignore) negative values of phase in averaging across bands. Negative phase values are removed only for frequencies below the frequency given below, when calculating the average phase in bands. Default is TRUE.
- `remove_negative_phase_f_cutoff` The cut-off frequency below-which negative phase values are neglected (only if `remove_negative_phase` is TRUE). Default is 0.1.
- `normalize_ABP` Normalize ABP by dividing by the mean and multiplying by 100, to express ABP change in %. Note that mean-values are always removed from ABP prior to analysis. Default is FALSE.
- `normalize_CBFV` Normalize CBFV by dividing by the mean and multiplying by 100, to express CBFV change in %. Note that the band-average values of gain are always calculated both with and without normalization of CBFV, in accordance with the recommendations. Note also that mean-values are always removed from CBFV prior to analysis. Default is FALSE.
- `window_type` Chose window 'hanning' or 'boxcar'. Default is 'hanning'.
- `window_length` Length of the data-window, in seconds. Default is 102.4.
- `overlap` Overlap of the windows, in %. If `overlap_adjust` is TRUE (see below), then this value may be automatically reduced, to ensure that windows cover the full length of data. Default is 59.99% rather than 60%, so that with data corresponding to 5 windows of 100 s at an overlap of 50%, 5 windows are indeed chosen.
- `overlap_adjust` Ensure that the full length of data is used (i.e. the last window finishes as near as possible to the end of the recording), by adjusting the overlap up to a maximum value given by `params.overlap`. Default is TRUE.
- `na_as_mean` Changes all missing non-interpolated values to the mean value of the corresponding variable. This have not been adressed in the paper by Claassen, and to ensure the dataframes are not 'gathered' this should generate the most stable results. Default is TRUE.

## References

1. Claassen et al. (2016) J Cereb Blood Flow Metab. 2016 Apr;36(4):665-80. ([PubMed](#))

## Examples

```
data(tfa_sample_data)
TFA(tfa_sample_data[,c(1:3)], variables=c("abp","mcav"), freq=10)
```

---

tfa_sample_data	<i>TFA sample data</i>
-----------------	------------------------

---

## Description

Dataframe with data provided by Prof. Simpsons, with time (t), arterial blood pressure (abp), left MCAv (mcav\_l), right MCAv (mcav\_r), and end-tidal CO2 (etco2).



**Usage**

```
data(tfa_sample_data)
```

**Format**

An object of class "dataframe"; an example of the usage in [TFA](#)-function.

**Source**

[GitHub](#)

**References**

- Simpsons D (2015) ([Cerebral Autoregulation Research Network](#))
- Claassen et al. (2016) J Cereb Blood Flow Metab. 2016 Apr;36(4):665-80. ([PubMed](#))

**Examples**

```
data(tfa_sample_data)
TFA(tfa_sample_data[,c(1:3)], variables=c("abp", "mcav"), freq=10)
```

---

tfa\_sample\_data\_1      *TFA sample data - 1*

---

**Description**

Dataframe with data provided by Prof. Simpsons, with time (t), arterial blood pressure (abp), left MCAv (mcav\_l), right MCAv (mcav\_r), and end-tidal CO2 (etco2).

**Usage**

```
data(tfa_sample_data)
```

**Format**

An object of class "dataframe"; an example of the usage in [TFA](#)-function.

**Source**

[GitHub](#)

**References**

- Simpsons D (2015) ([Cerebral Autoregulation Research Network](#))
- Claassen et al. (2016) J Cereb Blood Flow Metab. 2016 Apr;36(4):665-80. ([PubMed](#))

**Examples**

```
data(tfa_sample_data)
TFA(tfa_sample_data_1[,c(1:3)], variables=c("abp", "mcav"), freq=10)
```

---

tfa\_sample\_data\_2      *TFA sample data - 2*

---

**Description**

Dataframe with data provided by Prof. Simpsons, with time (t), arterial blood pressure (abp), left MCAv (mcav\_l), right MCAv (mcav\_r), and end-tidal CO2 (etco2).

**Usage**

```
data(tfa_sample_data)
```

**Format**

An object of class "dataframe"; an example of the usage in [TFA](#)-function.

**Source**

[GitHub](#)

**References**

- Simpsons D (2015) ([Cerebral Autoregulation Research Network](#))
- Claassen et al. (2016) J Cereb Blood Flow Metab. 2016 Apr;36(4):665-80. ([PubMed](#))

**Examples**

```
data(tfa_sample_data)
TFA(tfa_sample_data_2[,c(1:3)], variables=c("abp", "mcav"), freq=10)
```

# Index

## \* datasets

- df.data1000, 6
- df.deleter, 7
- testdata10, 11
- tfa\_sample\_data, 16
- tfa\_sample\_data\_1, 17
- tfa\_sample\_data\_2, 18

clinmon, 2, 6, 7, 11

df.data10 (testdata10), 11

df.data1000, 6

df.deleter, 7

iscus, 7

ortable, 8

PLR3000, 9

print.rrGcomp (rrGcomp), 9

rrGcomp, 9

sRCT, 10

testdata10, 11

TFA, 12, 17, 18

tfa\_sample\_data, 16

tfa\_sample\_data\_1, 17

tfa\_sample\_data\_2, 18